# **Machine Learning Methods for Neural Data Analysis Demixing and Deconvolving Calcium Imaging Data**

Scott Linderman *STATS 220/320 (NBIO220, CS339N). Winter 2023.*



# **Announcements**

- Lab 1 due tomorrow at midnight.
	- Please upload **just the pdf** on Gradescope.
	- Please add a short paragraph at the end about **author contributions**
	- Please see Ed discussion for minor errata on Problems 2e and 3c.
- Lab 2 will be released tomorrow evening so you can read through it before the lab on Friday.
- Team assignments will be announced tomorrow night as well.

# **Agenda**

- 1. Optical physiology
- 2. Constrained Non-negative Matrix Factorization (CNMF)

- So far, we've study electrophysiological ("ephys") recordings with high density probes.
- The raw data is a **multidimensional time series** of **voltage measurements**, one for each recording site on the probe.
- When neurons near the probe fire an **action potential**, it registers a **spike in the voltage** on nearby channels.
- Typical recordings detect spikes from **O(100) neurons**.



20 ms

Array 1, day 58

### **Recap Electrophysiology**

- It's hard to detect neurons that fire rarely and produce low amplitude EAPs.
- More generally, you only pick up cells that happen to be close to the narrow probe.
- No cell-type specificity.
- In particular, ephys does not leverage our powerful genetic toolkits for certain model organisms.



20 ms

Array 1, day 58

### **Recap Electrophysiology Limitations**

### **Genetic tools Cre driver lines in mice**



g brain. Experiments include colorimetric in situ hybridization, fluorescent in situ hybridization and

oughout the brain. Enriched in restricted populations within the olfactory areas, piriform cortex, hippocampus, and in restricted populations of striatum, layer 5 neocortex, hypothalamus, pons and medulla. This is different from the ally expressed in layer 1.

4 and 5, septum, thalamus, and midbrain. In the cortex, unlike A930038C07Rik which is specifically expressed in layer 1, Creed in a scattered population of cells in layer 5.

ulations within the olfactory areas, hippocampus, striatum, thalamus, midbrain, pons, and medulla. Expression is scattered orter expression is widespread.

halamus.

he hypothalamus.

https://connectivity.brain-map.org/transgenic



### **Genetic tools GAL4 lines in flies**



https://www.janelia.org/node/45217



Split-GAL4 lines for MBONs



### **Genetically encoded indicators of neural activity How can we make cells fluoresce only when they spike?**

- 1. Look for a side effect of spiking.
- 2. Engineer a protein that fluoresces when that side effect is detected.
- 3. Modify the DNA of (subsets of) neurons to produce that protein.
- 4. Use a microscope to measure fluorescence in the genetically modified organism.



# **Genetically encoded calcium indicators (GECIs)**

- When neurons spike, voltage gated calcium channels (VGCCs) open and allow a rapid **influx of calcium ions** (Ca2+).
- Genetically encoded calcium indicators (GECIs) like **GCaMP** bind to these calcium ions and become fluorescent.
- The increased fluorescence decays as the calcium unbinds, producing a transient fluorescence indicative of neural spiking.
- Using driver lines, **GECIs can be targeted to specific cell types.**
- In some cases, **multiple GECIs** with different fluorescence wavelengths can be encoded simultaneously in different subpopulations.



Lin, Michael Z., and Mark J. Schnitzer. 2016. "Genetically Encoded Indicators of Neuronal Activity." *Nature Neuroscience* 19 (9): 1142–53.



# **Genetically encoded voltage indicators (GEVIs)**

- Calcium is an indirect measure of spiking. Genetically encoded **voltage indicators** modulate fluorescence as a function of membrane potential.
- **Lots of designs**: fusing voltage sensing domains (e.g. from voltage-gated ion channels) to fluorescent proteins; harnessing natural opsins from microbes or algae.
- GECIs are much more established, but great progress in GEVIs has been made in recent years.



Lin, Michael Z., and Mark J. Schnitzer. 2016. "Genetically Encoded Indicators of Neuronal Activity." *Nature Neuroscience* 19 (9): 1142–53.





# **Microscopy**

- Expressing the genetically encoded indicator is only half the battle.
- You still need to stimulate the cells with a light source and measure the resulting fluorescence.
- Again, there are lots of approaches: wide-field imaging, **2-photon microscopy**, laser scanning and spinning disk confocal microscopy, miniaturized GRIN lenses, fiber photometry.





Silasi et al. J Neurosci Methods. 2016



Svoboda and Yasuda. Neuron, 2006.





xy-Scan Scan lens

> Tube len Dichroic Objective Condenser

Mirror

[www.inscopix.com](http://www.inscopix.com)



http://zeiss-campus.magnet.fsu.edu/articles/spinningdisk/introduction.html

# **2 photon calcium imaging**





#### **2 photon calcium imagingOver 10,000 cells** 0.935 mm



Stringer et al, Nature 2019

# **Data analysis pipelines for 2P imaging**

CaImAn





- Modern packages like Suite2P and CaImAn go through a few key steps to extract fluorescence traces.
- The key challenges are:
	- Correcting for motion artifacts.
	- Separating overlapping cells.
	- Accounting for background fluorescence.
	- Deconvolving spikes from fluorescence traces.
- The brain is squishy and it moves in non-rigid ways in 3D during experiments.
- A variety of non-rigid motion correction algorithms have been proposed:
	- NoRMCorre (Pnevmatikakis and Giovannucci, 2017), used in CaImAn.
	- Phase correlation + kriging (Pachitariu et al, 2017) used in Suite2P.

#### reference image

a

 $\mathbf b$ 



patches



patch size overlap



#### difference with frame



#### upsampled patches







botl median<br>n of bot Rolling mean, i<br>or combination

# **Motion correction**



# **Data analysis pipelines for 2P imaging**







- Modern packages like Suite2P and CaImAn go through a few key steps to extract fluorescence traces.
- The key challenges are:
	- Correcting for motion artifacts.
	- Separating overlapping cells.
	- Accounting for background fluorescence.
	- Deconvolving spikes from fluorescence traces.

# Constrained Non-negative Matrix Factorization (CNMF)

# *Pnevmatikakis et al, Neuron 2016.*

- Model the motion corrected movie as a superposition of fluorescence traces from multiple neurons, plus background.
- We can pose this as another convolutional matrix factorization problem.
- **Punchline:** *it's nearly the same as what we did for spike sorting!*





# **CNMF**

- Let  $T$  denote the number of **frames** in the movie.
- denote the number of **pixels**. *N*
- *D* denote the duration (in frames) of a calcium spike.
- denote the (unknown) number *K* of **neurons** that generated the spikes.

# **Constants**





- **• Data:** 
	- Let  $X \in \mathbb{R}^{N \times T}$  denote the motion corrected and unraveled video.
- **• Latent Variables:** 
	- Let  $A \in \mathbb{R}_+^{K \times T}$  denote the time series of spike amplitudes for each neuron.
- **• Parameters:** 
	- Let  $\mathbf{W} \in \mathbb{R}^{K \times N \times D}$  denote the array of calcium responses for each neuron.

### **Data and Latent Variables**



#### Like last week, assume each spike induces a scaled calcium response in the video.  $[\mathbf{a}_k \otimes \mathbf{W}_k]_t + \mathbf{u}_0 \mathbf{c}_{0,t}, \sigma^2 \mathbf{I}$ )





$$
p(\mathbf{X} \mid \mathbf{A}, \mathbf{W}) = \prod_{t=1}^{T} \mathcal{N} \left( \mathbf{x}_t \mid \sum_{k=1}^{K} \left[ \mathbf{a}_k \otimes \mathbf{W} \right] \right)
$$

### **Probabilistic Model Likelihood**

• Assume the calcium responses factor into spatial and temporal components.

- Spatial factor  $\mathbf{u}_k$  specifies which pixels correspond to neuron  $k.$
- Constrain the temporal components to be exponential decays.

Time constant of the decay is a function of the indicator; O(100ms).

$$
\mathbf{W}_k = \mathbf{u}_k \mathbf{v}_k^\top
$$

$$
v_{k,d}=e^{-dl\tau}
$$

#### **Calcium response model**



$$
\mathbf{c}_{k,t} \triangleq [\mathbf{a}_k \otimes \mathbf{v}_k]_t = \sum_{d=0}^D a_{k,t-d} v_{k,d} = \sum_{d=0}^D a_{k,t-d} e^{-d/\tau}
$$

is the calcium trace of neuron  $k$ 

#### **Calcium response model**

# Then where  $[\mathbf{a}_k \otimes \mathbf{W}_k]_t = \mathbf{u}_k[\mathbf{a}_k \otimes \mathbf{v}_k]_t \stackrel{\Delta}{=} \mathbf{u}_k \mathbf{c}_{k,t}$





The calcium response can be written recursively, thanks to the **exponential response:**

**c***k*  $a_{k,t}$  $\overline{\mathbf{1}}$ 

$$
c_{k,t} = \sum_{d=0}^{D} a_{k,t-d} e^{-d/\tau}
$$
  
=  $a_{k,t} + \sum_{d=1}^{t-1} a_{k,t-d} e^{-d/\tau}$   
=  $a_{k,t} + \sum_{d=0}^{t-2} a_{k,t-(d+1)} e^{-(d+1)/\tau}$   
=  $a_{k,t} + e^{-1/\tau} c_{k,t-1}$ ,

Equivalently,  $a_{k,t} = c_{k,t} - e^{-1/\tau} c_{k,t-1}$ .

(Note, we took  $D \to \infty$  and zero-padded  $\mathbf{a}_k$  on the left.)

### **Recursive formulation**

In matrix form,

 $a_k = Gc_k$  **G** = 1 *e*−1/*<sup>τ</sup>*  $e^{-1/\tau}$  1 1

### **Recursive formulation**



Suppose  $a_{k,t} \sim \text{Exp}(\lambda)$ , as in the spike<br>sorting model.<br>*We* can derive the probability of  $\mathbf{c}_k$  using<br>change of measure formula, sorting model.

We can derive the probability of  $\mathbf{c}_k$  using the *k*

### **Via a prior on amplitudes Prior on calcium traces**

$$
p(\mathbf{c}_k) = \left| \frac{d\mathbf{a}_k}{d\mathbf{c}_k} \right| \prod_{t=1}^T \text{Exp}(c_{k,t} - e^{-1/\tau} c_{k,t-1})
$$

$$
= |\mathbf{G}| \prod_{t=1}^T \text{Exp}(c_{k,t} - e^{-1/\tau} c_{k,t-1})
$$









Since G is lower triangular, its determinant is the product of its diagonal; i.e. 1.

Thus,

### **Via a prior on amplitudes Prior on calcium traces**

**c***k*  $a_{k,t}$  $\overline{\mathbf{1}}$ 

$$
p(\mathbf{c}_k) = \prod_{t=1}^T \text{Exp}(c_{k,t} - e^{-1/\tau} c_{k,t-1}; \lambda)
$$

It's just the probabilities of the "jumps"  $a_{k,t}$ .

Following the same steps as last week, we end up with the following objective for optimizing the calcium traces:

*T* ∑  $t=1$  $(c_{k,t} - e^{-1/\tau} c_{k,t-1}),$ 

where

is the residual projected onto the spatial factor for this neuron.

$$
\mathscr{L}(\mathbf{c}_k) = -\frac{1}{2\sigma^2} ||\mathbf{c}_k - \boldsymbol{\mu}_k||_2^2 + \lambda \sum_{t=1}^k
$$

$$
\boldsymbol{\mu}_k = \mathbf{R}^\top \mathbf{u}_k
$$

# **Optimizing the calcium traces**

More compactly,

*T* ∑ *t*=1  $(c_{k,t} - e^{-1/\tau} c_{k,t-1})$ 

 $\mathbf{Gc}_k||_1$ .

$$
\mathcal{L}(\mathbf{c}_k) = -\frac{1}{2\sigma^2} ||\mathbf{c}_k - \boldsymbol{\mu}_k||_2^2 + \lambda \sum_{t=1}^k
$$

$$
= -\frac{1}{2\sigma^2} ||\mathbf{c}_k - \boldsymbol{\mu}_k||_2^2 + \lambda ||\mathbf{c}_k||_2^2 + \
$$

We still have that pesky hyperparameter  $λ...$ 

# **Optimizing the calcium traces**

$$
c_{k,t} = \frac{c_{k,t} - \mu_{k,t}}{\sigma} \sim \mathcal{N}(0, 1).
$$

### **Optimizing the calcium traces Dual formulation**

• Maximizing  $\mathscr L(\mathbf c_k)$  is equivalent to solving the following convex optimization problem,

for some threshold  $\theta$ .  $\hat{\mathbf{c}}_k = \arg \min_{\mathbf{c}_k} \quad \|\mathbf{G} \mathbf{c}_k\|_1 \quad \text{subject to} \quad \|\mathbf{c}_k - \boldsymbol{\mu}_k\|_2 \leq \theta, \quad \mathbf{G} \mathbf{c}_K \geq 0,$ 

- Under the model,  $c_{k,t} \mu_{k,t} \sim \mathcal{N}(0, \sigma^2)$ , and  $z_{k,t} = \frac{c_{k,t} r_{k,t}}{\sigma} \sim \mathcal{N}(0, 1)$ .
- $||z||_2$  is the norm of a vector of iid Gaussians. It follows a chi  $\chi$ ) distribution.
- Idea: for large  $T$ , the chi distribution concentrates around  $\sqrt{T}$ . So set  $\theta = (1+\epsilon)\sigma\sqrt{T}$ .
- How to get  $\sigma$ ? We can estimate the noise at each pixel by high-pass filtering the data, then standardize the data by dividing by the noise standard deviation so that in our model  $\sigma=1.$

- CVXPY is a powerful library for convex optimization in Python, based on the CVX package from Grant and Boyd.
- It's ideally suited to solving these types of problems.
- If you want to learn more, take Prof. Boyd's course, EE364, and read his book!

Stephen Boyd and Lieven Vandenberghe Convex Optimization



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#### Welcome to CVXPY 1.3

Convex optimization, for everyone.

We are building a CVXPY community on Discord. Join the conversation!

CVXPY is an open source Python-embedded modeling language for convex optimization problems. It lets you express your problem in a natural way that follows the math, rather than in the restrictive standard form required by solvers.

For example, the following code solves a least-squares problem with box constraints:

```
import cvxpy as cp
import numpy as np
# Problem data.
m = 30n = 20np. random. seed(1)A = np. random. randn(m, n)b = np. random. randn(m)# Construct the problem.
x = cp.Variable(n)objective = cp.Minimize (cp.sum_squares(A @ x - b))constraints = [0 \le x, x \le 1]prob = cp.Problem(objective, constraints)# The optimal objective value is returned by `prob.solve()`.
result = prob.solve()# The optimal value for x is stored in `x.value`.
print(x.value)# The optimal Lagrange multiplier for a constraint is stored in
# `constraint.dual_value`.
print(constraints[0].dual_value)
```




# **CVXPy**

- We typically constrain the **spatial factors to be non-negative** too, unlike in spike sorting.
- We need to account for **background fluorescence** from out-of-focus cells.
- Typically, assume **rank-1** or **spatially smooth** background. See notes.
- As always, **preprocessing is important** for finding candidate neurons and characterizing noise. More on this in the lab.



CNMF-E; Zhou et al, eLife 2018.

# **Miscellanea**



#### OnACID; Giovanucci et al, NIPS 2017. Mesoscope data from A. Tolias lab



CNMF-E; Zhou et al, eLife 2018. Very different background model required for 1p data

#### **Residual X 8**



# **Demixed** Time: 0.10 second

# **Conclusion**

- **Optical physiology** offers a powerful and complementary toolkit for measuring neural activity in genetically defined cells.
- Methods for extracting calcium fluorescence traces are very similar to those for spike sorting. It's all **convolutional matrix factorization with constraints.**
- If we have an estimate of the noise, we can use it to **set hyper parameters (i.e. thresholds) automatically**.
- **• Next time**: we'll dive deeper into the deconvolution problem of inferring spike times and amplitudes from calcium traces.

# **Further reading**

• Lin, Michael Z., and Mark J. Schnitzer. 2016. "Genetically Encoded Indicators of Neuronal Activity."

• Pnevmatikakis EA, Soudry D, Gao Y, et al. Simultaneous Denoising, Deconvolution, and Demixing

• Pachitariu, Marius, Carsen Stringer, Mario Dipoppa, Sylvia Schröder, L. Federico Rossi, Henry Dalgleish, Matteo Carandini, and Kenneth D. Harris. 2017. "Suite2p: Beyond 10,000 Neurons with

- Nature Neuroscience 19 (9): 1142–53.
- of Calcium Imaging Data. *Neuron*. 2016;89(2):285-299. doi:10.1016/j.neuron.2015.11.037
- Standard Two-Photon Microscopy." Cold Spring Harbor Laboratory. [https://doi.org/](https://doi.org/10.1101/061507) [10.1101/061507](https://doi.org/10.1101/061507).
- in Vivo Calcium Signals from Microendoscopic Video Data." eLife 7 (February): e28728.
- Analysis." eLife 8 (January). https://doi.org/10.7554/eLife.38173.

• Zhou, Pengcheng, Shanna L. Resendez, Jose Rodriguez-Romaguera, Jessica C. Jimenez, Shay Q. Neufeld, Andrea Giovannucci, Johannes Friedrich, et al. 2018. "Efficient and Accurate Extraction of

• Giovannucci, Andrea, Johannes Friedrich, Pat Gunn, Jérémie Kalfon, Brandon L. Brown, Sue Ann Koay, Jiannis Taxidis, et al. 2019. "CaImAn an Open Source Tool for Scalable Calcium Imaging Data

